

Hydrogels for Targeted Bone Formation

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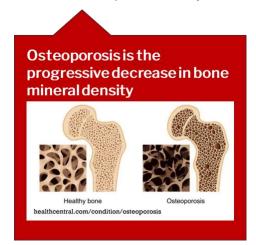
The Problem

1 in 2 women and 1 in 5 men over 50 years old sustain osteoporosis-related fracture

• Vertebral compression and hip (femur) fractures are most prevalent

~2% of Americans sustain a long-bone fracture in their lifetime

• Femur (300K hospitalizations/yr) and tibia/fibula (77K hospitalizations/yr) are most prevalent





Treatment Options

Surgery: internal/external fixation, replacement

Treatment Outcomes

- Disability ~50% of hip fractures
- Death ~25% of hip fracture patients within a year post-surgery
- Non-unions ~10% of long-bone fractures



Mission: to develop bone-producing materials that prevent (1) fracture & (2) non-unions







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Education and Training

- B.S., ChemE, Carnegie Mellon University, 2006
- B.S., BME, Carnegie Mellon University, 2006
- Ph.D., Chem & BiocheE, Rutgers University, 2014
- Postdoctoral Trainee, Bioengineering, University of Pennsylvania

Vega Lab Overview

- Over \$1.7M in funding from NIH, NSF, and Foundation Grants
- Inventor/co-inventor on 5 patent filings
- Lab has produced 16 publications & 2 additional under peer review
- Lab has presented 46 abstracts at regional and national conferences & presented at 18 invited talks
- Mentored/graduated 15 undergraduate students, 4 Master students, 2 Ph.D. students
- Lab personnel: 1 postdoc, 4 Ph.D. students, 12 undergraduate students
- Select awards: NSF CAREER (2023), NEBEC New Innovator (2023), CMBE Young Innovator (2022), ORS NIRA Finalist (2022)
- Served on NSF, NIH, and DoD review panels



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Education and Training

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- M.D., Albert Einstein College of Medicine, 2008
- Orthopaedic Surgery Resident, Hospital of the University of Pennsylvania, 2013
- Orthopaedic Oncology Fellowship, Memorial Sloan-Kettering Cancer Center, 2014

Orthopaedic Research Lab Overview

- Over \$460k in funding from DoD, and Foundation Grants
- Inventor/co-inventor on 1 patent filings
- Lab has produced 32 publications
- Lab has presented 51 abstracts at regional and national conferences & presented at 10 invited talks
- Mentored/graduated 11 medical students
- Lab personnel: 1 postdoc, 1 research manager, 3 M.D. students, 1 research assistant, 15 medical students, 3 undergraduate students
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RESEARCH ARTICLE

Bioscience

Self-Forming Norbornene-Tetrazine Hydrogels with Independently Tunable Properties

Kirstene A. Gultian, Roshni Gandhi, Tae Won B. Kim, and Sebastián L. Vega*

Although photopolymerization reactions are commonly used to form hydrogels, these strategies rely on light and may not be suitable for delivering therapeutics in a minimally invasive manner. Here, hyaluronic acid (HA) macromers are modified with norbornene (Nor) or tetrazine (Tet) and upon mixing click into covalently crosslinked Nor-Tet hydrogels via a Diels-Alder reaction. By incorporating a high degree of Nor and Tet substitution, Nor-Tet hydrogels with a broad range in elastic moduli (5 to 30 kPa) and fast gelation times (1 to 5 min) are achieved. By pre-coupling methacrylated HANor nacromers with thiolated peptides via a Michael addition reaction, Nor-Tet hydrogels are peptide-functionalized without affecting their physical roperties. Mesenchymal stem cells (MSCs) on RGD-functionalized Nor-Tet hydrogels adhere and exhibit stiffness-dependent differences in matrix mechanosensing. Fluid properties of Nor-Tet hydrogel solutions allow for injections through narrow syringe needles and can locally deliver viable cells and peptides. Substituting HA with enzymatically degradable gelatin also results in cell-responsive Nor-Tet hydrogels, and MSCs encapsulated in Nor-Tet hydrogels preferentially differentiate into adipocytes or osteoblasts, based on 3D cellular spreading regulated by stable (HA) and degradable

1. Introduction

Hydrogels are 3D and highly hydrated crosslinked polymer networks that are used in various biomedical applications including tissue engineering, drug delivery, and regenerative medicine.[1-5] To synthesize hydrogels, free-radical photopolymerization reactions using visible or ultraviolet light are commonly used due to are limited to either acellular or 2D cell culture. Alginate is an fast gelation under physiological conditions, (c) Depending on the anionic biopolymer that forms ionically crosslinked hydrogels moieties present, hydrogets can be formed via chain-growth or when mixed with divalent cations (e.g., Ca2+ or Zn2+),[15] Joni step-growth photopolymerization.[7,8] Free-radical chain-growth cally crosslinked hydrogels form rapidly, and alginate hydrogels photopolymerization of acrylated macromers form hydrogels

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in local differences in crosslink density, 17.9 which introduces heterogeneity that could unpredictably influence cell-hydrogel interactions of encapsulated cells. In contrast, free-radical step-growth photopolymerization between molecules containing thio and vinyl (ene) groups result in one-toone click reactions that form hydrogels with a homogenous network structure.17 Photopolymerized hydrogels have many advantages, including high biocompatibility and fast gelation times. Step-growth hydrogels also benefit from the potential for photopatterning which introduces heterogeneity to an otherwise homogeneous material.[10] Despite these advantages, freeradical photopolymerization reactions re quire light and thus are limited to applications where light is readily available or to applications where precise control of the gelation time is not needed.

Alternatives to hydrogel photopoly merization rely on other catalysts includ ing pH, electrostatic interactions, and temperature.[11] For example, Michael-

addition reactions between thiols and acrylates form hydrogels with tunable mechanical properties, and gelation rates can be decreased with increasing pH.[12,13] Michael-addition reactions are robust, and have been used to form hydrogels for static and dynamic 2D cell culture studies.[14] However, due to slow gelation times and the need for high pH buffers, these hydrogels specifically have been extensively used for tissue engineering and cellular delivery applications. [16] Despite their high biocompatibility and ease of use, ionically crosslinked hydrogels generally feature low mechanical properties and are unstable due to the diffusion of divalent cations over time.

Thermoresponsive hydrogels are another class of hydrogels that transition from liquid to hydrogel above a lower critical solution temperature (LCST) or below an upper critical solution temperature (UCST).[17,18] For example, Sala et al. developed there mosensitive poly(N-vinylcaprolactam) (PNVCL) hydrogels that are liquid at room temperature and gel at a physiologic LCST[19] Chondrocytes and mesenchymal stem cells (MSCs) encapsulated in these hydrogels exhibit high viability and cartilage extracellular

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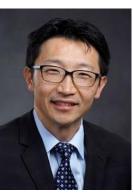
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Injectable hydrogel with immobilized BMP-2 mimetic peptide for local bone

regeneration Kirstene A. Gultian¹, Roshni Gandhi¹, Kayla DeCesari¹,

Vineeth Romiyo2, Emily P. Kleinbart2, Kelsey Martin2, Pietro M. Gentile², Tae Won B. Kim^{1,2} and Sebastián L. Vega^{1*}

Osteoporosis is a disease characterized by a decrease in bone mineral density thereby increasing the risk of sustaining a fragility fracture. Most medical therapies are systemic and do not restore hone in areas of need, leading to undesirable side effects. Injectable hydrogels can locally deliver therapeutics with spatial precision, and this study reports the development of an injectable hydrogel containing a pentide mimic of hone mornhogenetic protein-2 (RMP-2). To create injectable hydrogels, hyaluronic acid was modified with norbornene (HANor) or tetrazine (HATet) which upon mixing click into covalently crosslinked Nor-Tet hydrogels. By modifying HANor macromers with methacrylates (Me), thiolated RMP-2 mimetic pentides were immobilized to HANor via a Michael addition reaction, and coupling was confirmed with 1H NMR spectroscopy. BMP-2 peptides presented in soluble and immobilized form increased alkaline phosphatase (ALP) expression in MSCs cultured on 2D and encapsulated in 3D Nor-Tet hydrogels. Injection of bioactiv Nor-Tet hydrogels into hollow intramedullary canals of Lewis rat femurs showed a local increase in trabecular bone density as determined by micro-CT imaging. The presented work shows that injectable hydrogels with immobilized BMP-2 peptides are a promising biomaterial for the local regeneration of bone tissue and for the potential local treatment of osteoporosis

osteoporosis, injectable hydrogels, hyaluronic acid, BMP-2, DWIVA peptides, bon

1 Introduction

Osteoporosis is characterized by a reduction in bone mineral density and disruptio of bone microarchitecture (Wright et al., 2014). Osteoporosis is the most comm chronic metabolic bone disease with an estimated 200 million people affected worldwide (Sozen et al., 2017). According to the International Osteoporosis Foundation, 1 in 3 women above the age of 50 and 1 in every 5 men will experience fragility fractures resulting from osteoporosis in their lifetime (Cooper, 1999). Osteoporosis increases the

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Education and Training

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MSTS and AAOS review panels

















Our Solution

Objective

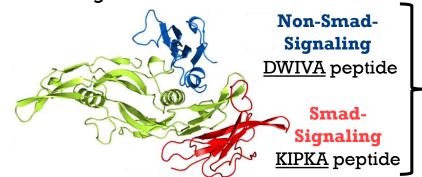
To deliver <u>therapeutics</u> via an injection that locally form bone at the injection site.



- Preventative: strengthen bone prone to fracture due to osteoporosis and/or prevent non-unions
- Accelerated healing: Improve healing of non-unions

Bone morphogenetic protein-2 (BMP-2)

FDA-approved protein used for spine fusion and non-union surgeries.



BMP-2
peptides
are robust,
specific & can
reduce offtarget effects of
BMP-2 proteins

Bone Morphogenetic Protein-2 (osteoinductive protein = causes bone formation)

- Postoperative inflammation
- Ectopic bone formation
- Hyperactive osteoclast-mediated bone resorption





Our Solution: HydroBone

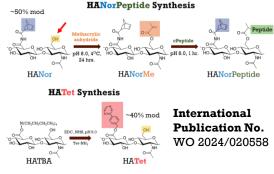
- HydroBone is a self-forming hydrogel injection that <u>locally</u> delivers BMP-2 peptides
- HydroBone can control BMP-2 signal dosing/presentation and thereby reduces offtarget effects of BMP-2 proteins

Self-forming hydrogel injection



Gultian+ Macromolecular Bioscience 2023

Hydrogel functionalization with BMP-2 peptides



Gultian+ Macromolecular Bioscience 2023

Hydrogels induce bone formation at injection site (femur)



Gel (G)





Gultian+ Frontiers in Biomaterials Science 2022 Love+ Journal of Orthopaedic Research 2024





Market Opportunity

- Preventative (osteoporosis) & interventional (long-bone fracture)
 market: \$28+ billion/yr
 - Osteoporosis therapeutics market valued at \$13.06 billion in 2022 & predicted to reach \$20.53 billion by 2032, growing at a CAGR of 4.7% (Emergen Research)
 - Fracture fixation market was valued at \$15 billion in 2022 and is predicted to reach \$22.51 billion in 2028, growing at a CAGR of 7.0% (Business Research Insights)
- Serviceable Available Market: \$5.7+ billion/yr
 - 1.3 million long bone fractures * \$2500 per case = \$3.25 billion/yr
 - 600,000 delayed healing (non-union) fractures * \$2500 per case = \$ 1.5 billion/yr
 - 400,000 arthrodesis (fusion) procedures per year * \$2500 per case = \$1 billion/yr





Summary



We developed **HydroBone**, an injectable hydrogel that delivers BMP-2 peptides

Three applications:

- Prevent osteoporosis-related bone fracture by injecting HydroBone to areas prone to fracture (femur, lumbar vertebra)
- **2. Prevent non-unions** by injecting HydroBone to long-bone fractures during surgery
- Improve healing of non-unions of long bone fractures

Received pre-seed funding from Foundation Venture Capital Group to evaluate the effects of HydroBone in bridging a non-healing femur segmental defect

Experimental Design



- Stabilize femur with external fixator plate (RISystem)
- 2. Create non-healing defect in the femur (5 mm)
- 3. Treat defect with one of 5 groups:
 - Sham (defect, no intervention)
 - Gel (no peptides)
 - Gel +KIPKA peptide [at dose shown to maximize Smad-dependent signaling in vitro]
 - Gel +DWIVA peptide [at dose shown to maximize Smad-independent signaling in vitro]
 - Gel +rhBMP2 protein

Measurable Outcomes: goals are to (1) confirm signaling pathway in vivo and (2) demonstrate endochondral ossification during bone healing.

- 1. 1-week post-op: targeted BMP-2 mediated signaling [histology]
- 2-weeks post-op: soft callus formation [histology]
- 3. 4-weeks post-op: hard callus formation [histology, µCT]
- 8-weeks post-op: bone remodeling/homeostasis [histology, µCT, biomechanical testing]





Thank You & Happy to Take Questions!



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